A semi-automated method for measuring thickness and white matter integrity of the corpus callosum

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Many diseases affect human brain white matter, multifocally or diffusely, in adults and children. These may be metabolic (e.g. Leigh's disease), toxic (e.g. carbon monoxide poisoning), hypoxic (e.g. hypoxic ischaemic injury), infective (e.g. HIV or syphilis), inflammatory (e.g. multiple sclerosis) or vascular (e.g. microvascular dementia). Two important conditions that result in significant loss of global white matter volume in affected children are hypoxic ischaemic injury and HIV encephalopathy. These diseases result in the thinning of associated fibre bundles and may be reflected by atrophy of inter-hemispheric connections – most importantly the corpus callosum (CC) (Fig. 1).

A simple automated method of determining normal values of the CC according to age is desirable. A tool which is also applicable for diagnosing white matter disorders and offering prognosis in children with global white matter insults will have a wide clinical application. This article describes a semi-automated system that divides the midline CC into a number of segments and determines thickness at each, then performs fibre tracking from these segments.

Aim. Diseases affecting cerebral white matter may lead to left-right asymmetries and atrophy of interhemispheric connections, i.e. the corpus callosum (CC). Our aim was to describe and test a semi-automated system that divides the midline CC into a number of segments and determines thickness at each, then performs fibre tracking from these segments.

Methods. Six normal female volunteers (average age 25.8 ± 6.7 years) and a female patient with diagnosed multiple sclerosis (age 26 years) were scanned on a 3T MRI. We performed diffusion-weighted imaging in 12 directions, and calculated diffusion tensors and fractional anisotropy (FA) maps from this pre-processed data. Fibre tracking from a region-of-interest encompassing the entire CC was done. This fibre data, together with FA maps and the unweighted diffusion tensor imaging (DTI) image (b = 0 s/mm²), were imported into a custom tool written in MATLAB. The midline sagittal position was carefully defined by selecting multiple midline points in coronal and axial views and rotating the image volume and fibre co-ordinates accordingly.

Using the customised tool, dorsal and ventral CC contours were manually drawn on the mid-sagittal FA image, initiating automated calculation of a contour midway between these manually drawn lines. The programme was designed to then divide the midline contour into a pre-selected number of segments; from each segment border, perpendicular spokes were projected until they intersected with the dorsal and ventral contours. This technique divided the CC into a pre-set amount of segments, the number of which was limited by the spatial resolution. It was decided to set the number at 40 to ensure that each segment depicted a contiguous strip of voxels across the CC from the dorsal to the ventral contour. The system allows these segments to then be used as seeds for separate fibre tracking in each cerebral hemisphere, and various parameters are automatically plotted as a function of distance along the midline contour. The following parameters are measurable: midline CC thickness; midline FA; fibre volume for each hemisphere (represented as a left/right ratio centred on zero) and mean fibre FA for each hemisphere (also represented as a left/right ratio centred on zero).

Results. The tool proved successful in measuring and plotting CC midline thickness and FA, but was not sensitive for peripheral white matter lesions.

Conclusions. The technique successfully determined values of CC midline thickness, FA and interhemispheric differences. Future research will determine normal values for age and compare CC thickness with peripheral white matter volume loss in large groups of patients, using the semi-automated technique.
Methodology

Six normal female volunteers (average age 25.8 ± 6.7 years) and a 26-year-old female patient with diagnosed multiple sclerosis (MS) were scanned on a 3T MRI system (MAGNETOM Allegra, Siemens, Erlangen). Informed consent was obtained and protocols were approved by the Stellenbosch University Ethics Committee.

Diffusion-weighted imaging was performed in 12 directions with a b-value of 1 000 sec/mm$^2$, and one volume was acquired with b = 0 sec/mm$^2$. Other parameters included:

- field of view (FOV) = 240 mm
- spatial resolution = 1.9 x 1.9 mm$^2$
- slice thickness = 1.9 mm
- matrix size = 128 x 128 pixels
- slices = 75
- TR = 10 400 ms
- TE = 86 ms.

Five identical acquisitions were taken, and were averaged after eddy correction and outlier rejection. Co-registration was then performed across the 5 averages using affine transformations, with the unwighted image of the first average as a reference. Diffusion tensors and fractional anisotropy (FA) maps were then calculated from these pre-processed data.

From a region-of-interest encompassing the entire CC, fibre tracking was done using fibre assignment by continuous tracking (FACT) in DTIStudio (Jiang and Mori, Johns Hopkins University, 2007). The FA tract initiation and termination threshold was 0.2, and the principle eigenvector angle stopping criterion was 70°. Extraneous fibres, such as those projecting down into the spinal cord, were removed. This fibre data, together with FA and the unweighted diffusion tensor imaging (DTI) image (b = 0 s/mm$^2$), were imported into a custom tool written in MATLAB (The Mathworks Inc, Natick, MA). The midline sagittal position was carefully defined by selecting multiple midline points in coronal and axial views, and rotating the image volume and fibre co-ordinates accordingly.

Using the customised tool, dorsal and ventral CC contours were manually drawn on the mid-sagittal FA image. This initiated the automated calculation of a contour midway between the manually drawn lines. The programme was designed to then divide the midline contour into a pre-selected number of segments, from the borders of which perpendicular spokes were projected until they intersected with the dorsal and ventral contours. This in turn divided the CC into a preset number of segments (Fig. 2). The number of segments was limited by the spatial resolution, and it was decided that having 40 segments would ensure that each one still contained a contiguous strip of voxels across the CC from the dorsal to the ventral contour.

Results

Fig. 4 shows the various parameters successfully determined from the MS patient, plotted as a function of normalised distance along the CC midline. The various parameters are automatically plotted as a function of distance along the midline contour. The following parameters are measurable:

- midline CC thickness
- midline FA
- fibre volume for each hemisphere (represented as a left/right ratio centred on zero)
- mean fibre FA for each hemisphere (also represented as a left/right ratio centred on zero).

With this system, the segments can be measured (representing the CC thickness at several locations) and used as seeds for fibre tracking separately in each cerebral hemisphere (Fig. 3). The various parameters are automatically plotted as a function of distance along the midline contour. The following parameters are measurable:
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dotted lines provide a normal range (defined as the mean ± 1 standard deviation of the corresponding parameters) successfully determined from the 6 normal subjects. To simplify interpretation but still preserve the trend details, these normal bounds have been smoothed using a 6th order polynomial.

Discussion

The CC is the main inter-hemispheric commissure of the brain. It plays a role in unifying sensory fields, organising bimanual motor output, aiding memory storage and retrieval, allocating attention and arousal, facilitating language and auditory functions, and in consciousness itself. For pathologists and radiologists alike, however, the ability to evaluate the volume and integrity of white matter has been notoriously elusive. Now, DTI fibre tracking, and DTI-derived metrics such as FA, provide a means for measuring and demonstrating white matter features. DTI fibre tracking can be used to associate known anatomical landmarks (such as the CC) with regions where localisation may be ambiguous (such as off-midline, or peripheral, hemispheric white matter).

The midline sagittal view of the CC has been parcellated in a variety of ways according to both structural geometry and function. DTI fibre tracking has already been used in this context to segment the CC into bands corresponding to structural and functional units. CC thickness in the sagittal plane has been shown to be associated with a variety of factors including better motor performance and with verbal IQ and fluency. The CC thickness may be secondarily affected by fibre loss, as seen in children after severe hypoxic ischaemic injury, HIV encephalopathy or large infarcts.

The semi-automated system that we designed (as described above) was tested successfully and allowed measurement of midline CC, midline FA, mean fibre FA for each hemisphere and fibre volume for each hemisphere for all 7 adults. These were plotted by the system as graphs demonstrating the ability to determine ranges of normal values. This would be suitable for use in children, to determine age-related differences in myelin maturation and volume. The technique can now also be used to compare CC thickness with hemispheric brain volume in both normal children and those with cerebral atrophy, such as seen with hypoxic ischaemic injury and HIV encephalopathy. Observations can then be correlated with functional scores and used for predicting outcome and function. In addition, cases in which patients with HIV are receiving antiretroviral therapy can be followed up to determine if the patients regain white matter volume and CC thickness.

For the patient with MS, we anticipated a thinning of the CC or decrease in midline FA. A previous study by Dorion et al. shows the total size of the CC in females to be unrelated to hemispheric asymmetry. In our patient, differences in CC thickness (Fig. 4a) were too large to be accounted for by differences in midline contour length. Although regional decreases in FA in normal-appearing white matter have been shown in the CC of MS patients, there is no clear indication thereof in Fig. 4b.

On a macro-scale, a healthy brain is largely symmetrical across the mid-sagittal plane. However, the ratio of grey to white matter is smaller in the right hemisphere than in the left, and numerous regional interhemispheric asymmetries have also been identified. Of these inter-hemispheric differences, regions that the CC fibres are likely to cross include frontal areas (where the right volume is greater than the left) and
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